

Longitudinal CT scanning for explainable early detection of postharvest disorders: The ‘Braeburn’ browning case

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Abstract

Longitudinal computed tomography (CT) datasets quantify the internal state of agricultural products in 3D over time, making them very suitable for studying the progression of postharvest disorders. In this paper, we present a workflow for developing early detection systems using longitudinal CT datasets. In our workflow, each CT-voxel is treated as a time series, which facilitates the analysis and detection of gradually progressing disorders in four different ways. Firstly, visualizing the difference between two CT scans provides higher contrast visualizations to study the progression of a disorder. Secondly, features derived from regional changes can be more discriminative than features derived at one time point over the whole product. Thirdly, detection setups can be simulated at different scanning times, making it possible to compare potential factory setups. Fourthly, longitudinally explainable artificial intelligence answers a specific research question about the decision-making of a neural network. The workflow is showcased on a dataset of CT scans of 80 ‘Braeburn’ apples that developed core browning. We provide a detailed visualization of the progression of core browning during and after controlled atmosphere (CA) storage. Moreover, a deep neural network classifier was developed that had more than 90% accuracy in the early detection of browning. The presented workflow provides powerful tools to study and automatically detect disorders that develop over time, thereby aiding in waste reduction and marketability.

Keywords: non-destructive testing (NDT), image registration, apple, internal browning, explainable artificial intelligence (XAI), integrated gradients

1 Introduction

Roughly one-third of the food produced for human consumption is wasted globally (Gustavsson et al. 2011). Sorting agricultural products based on non-destructive measurements can reduce waste and improve customer satisfaction (Nicolai et al. 2014). X-ray imaging can be used to determine the internal quality of a product, such as the presence of internal disorders (Kotwaliwale et al. 2014). The two main X-ray imaging methods are radiography, which is faster and cheaper, and computed tomography (CT), which has higher contrast and allows imaging in 3D. Radiographs can be simulated from CT scans (Hendriksen et al. 2021), so a CT dataset can be used to study both CT and radiography.

Many internal disorders develop gradually, so multiple scans over time may be acquired to study the progression of these disorders (Lammertyn et al. 2003; Jarolmasjed et al. 2016). A dataset is longitudinal when the same samples were measured multiple times. With longitudinal datasets, it is possible to separate the natural variance in the products from the changes over time (Tijskens et al. 2015). Image registration (Zitova and Flusser 2003) can be used to align the orientation of CT scans after acquisition. Image registration has been used to provide precise side-by-side views (Muziri et al. 2016) or to calculate how much a sample changed over time (Van Dael et al. 2019). Outside of agriculture, the difference between two images (a difference image) has been used for higher contrast visualizations of medical scans (Newatia et al. 2007) and for detecting supernovae in astronomy (Zackay et al. 2016).

For gradually developing disorders early detection is valuable. Early detection can limit infectious disorders from spreading such as fruit flies (Yang et al. 2006). Moreover, some foods are still consumable if a disorder is detected at an early stage, but not at a later stage, such as apples with bitterpit (Jarolmasjed et al. 2016), or pears with mealiness (Muziri et al. 2016). Core browning is a common (Argenta et al. 2021) internal disorder in apples that is induced by controlled atmosphere (CA) storage, and continues developing out-of-storage (Watkins and Mattheis 2019). Apples are typically sorted immediately after CA storage, and the browning may develop further in the time between sorting and consumption. Therefore, browning must be detected at a very early stage to avoid brown apples reaching the consumer.

In recent years, many authors have reported successes in the application of deep learning methods to detect postharvest disorders (Tempelaere et al. 2023a). Deep learning has been applied on CT scans of many crops such as apples (Tempelaere et al. 2024), pears (Van de Looverbosch et al. 2021; Tempelaere et al. 2023b), avocado (Andriiashen et al. 2023; Matsui et al. 2023), mango (Ansah et al.

2023) and passion fruit (Lu et al. 2023). Deep learning models are 'black box' models, meaning that their inner workings are too complex to interpret directly by humans. Explainable artificial intelligence (XAI) methods have been developed to gain insight into how neural networks interpret images (Buhrmester et al. 2021). Different XAI methods exist that highlight different parts of the image and it is challenging to evaluate how well they perform (Hooker et al. 2019). To counter the evaluation problem Sundararajan et al. (2017) formalized axioms that an XAI technique should follow, and derived a technique called integrated gradients (IG) directly from these axioms.

In this paper, we present a workflow for using longitudinal CT datasets to develop early detection systems for postharvest disorders. The key contribution of this paper is showing that image registration of the CT scans makes it possible to treat individual voxels as longitudinal data, and that this benefits the development of X-ray-based early detection systems in four ways. 1. Improved contrast of visualizations. 2. More discriminative features for quantitative analysis. 3. Early detection classifiers can be compared. 4. More interpretable explainable AI.

As an example case of our workflow, we studied core browning in 'Braeburn' apples. To capture the entire development of the disorder, 359 CT scans of apples were acquired before, during, and after CA storage. The severity of browning was scored at the end of the shelf life period using destructive visual inspection. With our workflow, we developed deep neural networks that were capable of scoring the browning severity of apples on a 1-4 scale, and performing early detection of browning on the day that apples were taken out of CA storage.

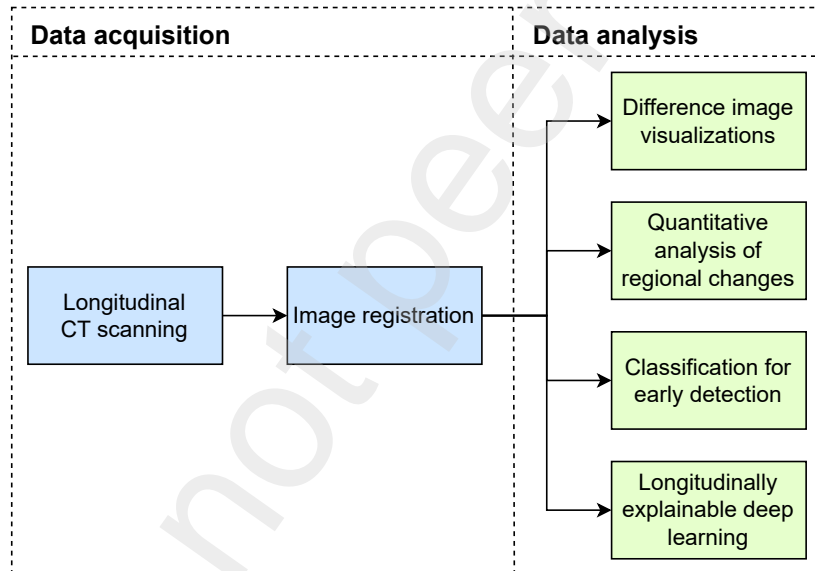


Figure 1: Overview of our workflow.

2 Workflow overview

Our workflow for developing early detection systems using longitudinal CT scanning consists of two data acquisition steps, and four methods that can be used to analyse the data (Figure 1). The ordering of the data analysis methods in Figure 1 relates to the different stages in developing an early detection system: First, visual inspection of the data is performed, then quantitative evaluation is performed, after that, an automatic detection system is developed, and finally, the automatic detection system is evaluated. We show in our results that image registration and longitudinal CT scanning provide added value in all these stages of development. A short description of each part of the workflow is provided below.

Longitudinal CT scanning. To acquire a longitudinal dataset, the same products must be scanned multiple times. The longitudinal CT dataset describes the progression of the disorder over time in 3D.

83 **Image registration.** Image registration should be used to align the orientation of the CT scans.
84 After image registration, individual voxels can be treated as longitudinal data, which is required
85 by the data analysis methods in our workflow.

86 **Difference Image visualizations.** A difference image results from subtracting two registered im-
87 ages of the same subject. The difference image will be zero on areas that are the same between
88 both images and non-zero for areas that have changed. It can greatly improve the visibility of
89 small changes on a static background (Newatia et al. 2007; Zackay et al. 2016). By subtracting
90 the first CT scan from later CT scans the changes to the product can be visualized at each
91 stage of the disorder.

92 **Quantitative analysis of regional changes.** Many features can be derived from CT datasets.
93 The value of a feature varies because of the natural variation of an object, and because of
94 the developments over time. By calculating the difference of a feature between two time points
95 the effect of the natural variation can be eliminated (Tijssens et al. 2015). Moreover, if it
96 is known that a disorder mostly affects a specific region features can be calculated only over
97 that region. These two approaches can be combined to derive more discriminative features for
98 quantitative analysis of disorders.

99 **Classification for early detection.** CT scans can be used to simulate arbitrary X-ray imaging
100 geometries (Hendriksen et al. 2021). Classifiers (e.g. deep neural networks) can be trained on
101 the simulated data. This makes it possible to compare potential factory X-ray imaging setups
102 without having to acquire the same dataset multiple times with different hardware. With
103 longitudinal datasets, it is possible to train classifiers to predict the state of the disorder at a
104 later time point in the dataset.

105 **Longitudinally explainable deep learning.** Explainable AI (XAI) techniques aim to describe an
106 AI’s decision-making by scoring how much each input feature attributed to the AI’s decision.
107 The integrated gradients XAI technique (Sundararajan et al. 2017) can be used with a longitu-
108 dinal baseline (Mamalakis et al. 2023) to answer the question: “How much did each change in
109 the product over time affect the classification score over time?”

110 3 Methods

111 In this section, we describe how our workflow was applied in practice to a dataset of ‘Braeburn’ apples
112 to develop an early detection system for core browning. All computational methods were implemented
113 using scripts in the Python programming language. The Python code is publicly available on Github
114 (https://github.com/Dirk123/longitudinal_ct_workflow).

115 3.1 Longitudinal CT scanning

116 3.1.1 Apple samples

117 In 2022, 80 ‘Braeburn’ apple fruit were harvested at the optimal harvest date from the Randwijk
118 experimental orchard, the Netherlands. To cause browning to develop, the apples were stored in
119 controlled atmosphere (CA) storage with non-optimal conditions (0.5 °C, 1.5 kPa O₂, 5 kPa CO₂).
120 The apples were stored in CA storage for 9, 12, or 17 weeks. After CA storage, the apples were
121 stored in shelf-life conditions (19-20 °C) for up to three weeks. Varying durations of CA and shelf-life
122 storage were used to ensure variety in the browning severity. Moreover, due to the scanning time and
123 the availability of the scanner, not all apples were scanned at each interval. An overview of the scans
124 is provided in Table 1. After the last CT scan the fruit were sliced with a knife into approximately
125 10 mm slices, photographed, and scored for browning intensity. Browning intensity was scored for
126 each browning type on a subjective scale of 1 to 4, where; (1) indicates no brown tissue; (2) mild; (3)
127 moderate and (4) severe browning intensity. One apple was excluded because it developed severe rot.
128 A part of this dataset was used in a previous publication within the same research project (Wood
129 et al. 2024).

Table 1: Overview of when the apples were scanned and sliced. When apples were sliced, they were scored on their level of browning.

CA storage (weeks)	Shelf-life (days)	Scanned	Sliced	Healthy	Brown	Excluded (rot)
0	0	32	-	-	-	-
3	0	10	1	1	0	0
9	0	21	-	-	-	-
	14	8	5	4	1	0
	21	3	3	1	2	0
12	0	30	3	3	0	0
	2	27	-	-	-	-
	9	27	-	-	-	-
	14	27	27	15	12	0
17	0	41	-	-	-	-
	2	41	-	-	-	-
	4	31	-	-	-	-
	7	41	21	5	15	1
	14	20	20	3	17	0
Totals		359	80	32	47	1

3.1.2 CT scanning protocol

The apples were scanned at the FleX-ray laboratory (Coban et al. 2020) using a custom scanner developed by TESCAN-XRE, Gent, Belgium. A cone beam geometry with a circular trajectory was used to acquire 1440 projection images at an exposure time of 100 ms, a tube peak voltage of 90 kV, and a current of 550 μ A. A detector pixel binning of two was used and the voxel size was between 130.6 μ m and 134.3 μ m. The voxel sizes differed slightly between scans due to one scanner motor being defective on some scan days, which limited the range of possible resolutions but otherwise did not affect the scans. The average time per scan was five minutes.

3.1.3 Image reconstruction

The FDK algorithm (Feldkamp et al. 1984) was used for reconstructing the CT volumes. Third-order polynomial beam hardening correction was used (Herman 1979), using a paper cup filled with apple juice as a calibration phantom. Gradient descent with momentum was used to optimize the beam hardening parameters (Schoonhoven et al. 2024). The cost function was the mean squared error (MSE) between each voxel inside the juice and the mean value of that region plus the MSE between each voxel outside the cup and the mean value of that region. The gradient could be calculated automatically by using PyTorch autograd (Paszke et al. 2017) and the differentiable FDK implementation from the Tomosipo library (Hendriksen et al. 2021). The CT scan of a cup filled with juice was also used to normalize the CT gray values similarly to the porosity mapping method (Nugraha et al. 2019). In the remainder of the paper, a CT gray value of 1 represents a density equal to juice and a gray value of 0 represents a density equal to air.

3.2 Image registration

All CT scans were aligned in 3D to the first available CT scan of the same apple by using image registration with the SimpleITK library (Lowekamp et al. 2013; Avants et al. 2014). All apples were scanned with the stem on top, but the rotation around the stem-calyx axis differed between scans. To avoid converging to the wrong local minimum, the first optimization step of the registration method was performed ten times with a different initial rotation. The initial rotations were equally spaced between 0 and 360 degrees around the vertical axis. In this first step, a rigid transformation model was optimized over the MSE using the L-BFGS optimizer (D. C. Liu and Nocedal 1989) with four and two times downsampling. The image registration parameters with the lowest MSE were used as initialization for the second step. In the second step, a similarity transformation model was optimized over the MSE using the regular step gradient descent optimizer with four times, two times, and no

161 downsampling.

162 3.3 Difference image visualizations

163 Difference images were calculated between the CT slices of the before-storage scan and all other scans
164 of the same apple, to visualize which parts of the apple changed during CA storage. Difference images
165 were also calculated from simulated radiographs. The radiographs had to be simulated because the
166 image content of radiographs acquired at different angles is different, and therefore they could not be
167 aligned with image registration. The radiographs were simulated from the registered CT scans using
168 the Tomosipo Python library (Hendriksen et al. 2021).

169 3.4 Quantitative analysis of regional changes

170 3.4.1 Image segmentation

171 Image segmentation was performed to segment the apple into the core, inner apple, outer apple,
172 and background. The aim was to be able to select the inner region as this is where core browning
173 occurs and to separate it from the core and the outer regions. Figure 2 shows an example of the
174 segmentation. The first available scan of each apple was segmented and these segmentation masks
175 could also be used on the other scans of the same apple because all scans were aligned after the image
176 registration.

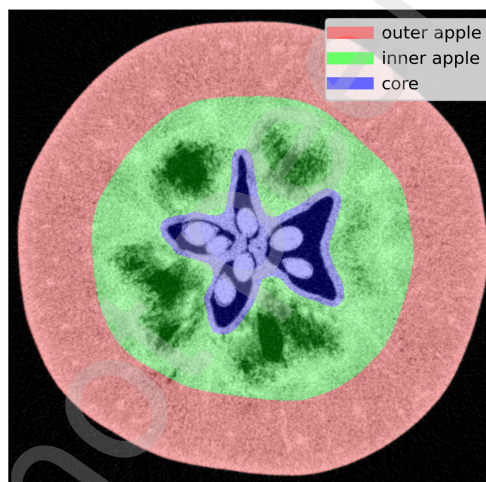


Figure 2: Example of the segmented regions.

177 To segment the full apple from the background, the CT scan was thresholded at 0.4. Morphological
178 closing and hole filling were used as postprocessing to ensure the whole volume was included. To
179 segment the apple core, only a central part of the CT scan was considered: 20 % above and below the
180 center of mass vertically and the central 50 % of the image horizontally. Within this region, voxels
181 below a threshold of 0.15 were selected as an initial estimate of the core. This mask was refined by
182 using binary dilation, selecting the largest connected component, binary closing, and hole filling using
183 Scikit-image (Walt et al. 2014). The outer apple region was defined as the region inside the apple at
184 most 12 mm from the peel. The inner apple region was defined as the rest of the inside of the apple
185 except the core region.

186 3.4.2 Porosity over time

187 The porosity is defined as the percentage of volume consisting of voids in a given region (Mendoza
188 et al. 2007). CT scans can be interpreted as maps of local porosity using porosity mapping (Nugraha
189 et al. 2019). To perform porosity mapping the CT scan needs to be corrected for beam hardening, and
190 the range of values needs to be normalized to the density of juice, which was performed as described

191 in Section 3.1.3. A local estimate of the porosity p of a voxel can be derived from the juice equivalent
192 density d as follows:

$$p = 1 - d$$

193 The local porosity estimates were averaged over the whole apple and the inner apple region to estimate
194 the porosity of these regions.

195 3.4.3 Statistical differences between browning scores

196 Statistical testing was performed to check if the porosity was significantly different for apples with
197 different browning scores. Four porosity-related features were calculated: The whole apple and inner
198 apple porosity on the last CT scan before slicing the apple, and their change from the before-storage
199 scan. The features were calculated on the 25 apples for which the before-storage scan was available
200 and which had been in CA storage for at least 12 weeks. Firstly, a one-way ANOVA test was
201 performed with the null hypothesis that the means were the same for all browning scores. Secondly,
202 a Tukey’s HSD test was performed to test if the difference between individual browning scores was
203 significant.

204 3.5 Classification for early detection

205 3.5.1 Comparing setups for detecting or predicting browning

206 Two tasks were investigated: to detect the browning score after shelf-life (detection), and to predict
207 the future browning score after CA storage but before shelf-life (prediction). For both tasks, neural
208 networks were trained on CT slices or real-time obtainable (100 ms) radiographs, so four neural
209 networks were compared. Only apples that had been in CA storage for at least nine weeks were
210 included. For the prediction networks, only apples that were sliced after two weeks of shelf life were
211 included. A 60%, 20%, 20% split was used between the training, validation, and test sets. The exact
212 number of images used can be found in Appendix A. Stratified sampling ensured each set contained a
213 similar ratio of apples from each day and with each browning label. For the test set, if possible, apples
214 were selected for which a before-storage scan was available, which was required for the explainable
215 AI method described in Section 3.6.2.

216 3.5.2 Training

217 The neural network training was implemented using Pytorch (Paszke et al. 2017) and Pytorch Light-
218 ning (Falcon and team 2024). The network architecture was a slightly modified version of the efficient-
219 netV2.s (Tan and Le 2021) implementation from torchvision (Marcel and Rodriguez 2010) pre-trained
220 on ImageNet-1K (Russakovsky et al. 2015). The weights of the original three input channels (RGB-
221 color) were averaged to obtain one grayscale input channel. Moreover, the network was converted to
222 a regression network by replacing the linear layer and the softmax activation function at the output
223 side of the network by a linear layer with one output. The cost function was the mean absolute
224 error (MAE). The optimizer was ADAMW (Loshchilov and Hutter 2017). Data augmentations were
225 applied using the Albumentations library (Buslaev et al. 2020) and the images were normalized based
226 on the mean and standard deviation of the training set. The training duration was approximately
227 20000 epochs (2 days on 2 RTX Titan GPUs). At the end of every epoch, the MAE was calculated
228 over the validation set, and the network weights were saved if the validation MAE was the lowest up
229 to that point. The version of the network with the lowest validation MAE at the end of the training
230 was used in the results section.

231 3.5.3 CT slices

232 For the networks trained on the CT scans, in every epoch, one horizontal slice was randomly selected
233 from the region 10% above or below the center of mass of the core of the apple, resulting in on average
234 123 slices being available per apple. The data augmentation consisted of random rotations, flipping,
235 shearing, translations, scaling, and elastic deformations (Simard et al. 2003).

3.5.4 Radiographs

The real radiographs that were acquired in the CT scanner were used for training the radiography neural networks. Flatfielding and the log-transformation were applied as preprocessing. To reduce storage space, only every third preprocessed radiograph was stored, resulting in 480 radiographs per apple. In every epoch, one radiograph was selected randomly per apple. The data augmentation consisted of random rotations, horizontal flipping, shearing, scaling, and elastic deformations (Simard et al. 2003). Moreover, 20% of the top and bottom of the radiograph were cropped to remove parts where browning does not occur.

3.5.5 Combining neural network outputs

For each apple multiple CT slices were available. These CT slices all had the same corresponding browning score. However, the scores outputted by the neural network were not always the same. The neural network outputs of all CT slices from one apple can be combined into a single score by taking the median. This way, errors in either direction cancel each other out, possibly improving the prediction of the browning score of the apple. This strategy was also applied to the radiographs. The MAE with the ground truth was calculated for all separate images and for the combined scores per apple. In both approaches, the score was rounded to the nearest integer before calculating the error.

3.6 Longitudinally explainable deep learning

3.6.1 Integrated gradients (IG)

To illustrate how the neural networks interpreted the X-ray images the integrated gradients (IG) (Sundararajan et al. 2017) explainable AI technique was used. The result of IG is a heatmap that highlights how much each part of the image has attributed to the browning score. To calculate this heatmap a second image is required that serves as a baseline. The choice of baseline image highly affects the outcome of IG (Sturmfels et al. 2020), and determines which research question is answered by the IG heatmap (Mamalakis et al. 2023).

There are several other techniques to calculate explainable AI heatmaps, but IG is unique in that it was designed to satisfy certain mathematical properties that make the heatmap more interpretable. Specifically, IG was designed to have the properties of sensitivity and implementation invariance. Sensitivity means that for every input and baseline that differ in one feature but have different predictions then the differing feature should be given a non-zero attribution. Implementation invariance means that the attributions are always identical for two functionally equivalent networks. Additionally, IG has the property of completeness, which means that the attributions add up to the difference between the output of (neural network) F at the input x and the baseline x' (Sundararajan et al. 2017).

3.6.2 Longitudinal baseline

Three baselines were compared in this paper. The constant black baseline (zero before normalization) was suggested in the original IG paper (Sundararajan et al. 2017). The constant zero baseline (zero after normalization) is the default of the Captum explainable AI library (Kokhlikyan et al. 2020), which was used to calculate the heatmaps. The registered before-storage scan was also used as a baseline (Mamalakis et al. 2023), which we will call the longitudinal baseline. Because of the completeness and sensitivity properties an IG heatmap shows how much the difference between the input and the baseline image affected the difference in neural network output between the input and baseline. For the longitudinal baseline this corresponds to the research question “How much did the changes in density from before storage affect the browning score?”

3.6.3 Augmentation based smoothing

To reduce noise and to avoid that the heatmap would be orientation dependent an augmentation-based smoothing procedure was applied similar to the method used by Gildenblat (2021). Multiple random affine and flipping augmentations were applied to both the baseline and the input image. The

284 range of transformations was the same as during the training of the neural networks. Heatmaps were
 285 calculated for the transformed baselines and inputs, and then transformed back to the original space
 286 by applying the inverse transformation. One hundred heatmaps were averaged to obtain a smoothed
 287 heatmap.

288 3.6.4 Evaluating the baselines

289 The output of the neural network on the baseline should stay close to the 1-4 range of scores, which
 290 we define as being within the [0.5, 4.5] range. Otherwise, the heatmap will mostly explain the baseline
 291 instead of the input image. This was checked for all three baselines.

292 Additional checks were performed to evaluate if IG with a longitudinal baseline could answer the
 293 research question “How much did the changes in density from before storage affect the browning
 294 score?” Browning will only increase over time. Therefore, on apples that did develop browning
 295 (ground truth score > 1) the neural network output should be higher on the input image than on the
 296 baseline. On the apples that did not develop browning (ground truth score 1), the networks should
 297 also score the baseline as healthy (within the [0.5, 1.5] range). These properties were tested for ten
 298 images per apple per network. The means and standard deviations over the network outputs were
 299 also calculated separately for the brown and healthy images.

300 4 Results

301 4.1 Difference image visualizations

302 Figure 3 shows CT scans, simulated radiographs, and their difference images visualizing brown core
 303 changes within one representative apple over time. Lower-density regions developed on the CT scan
 304 in the region around the core. The density in these regions decreased more after the apple was taken
 305 out of storage, than during storage. On the destructive visual inspection after the last CT scan this
 306 apple had severe browning (score 4). All apples with browning followed a similar pattern.

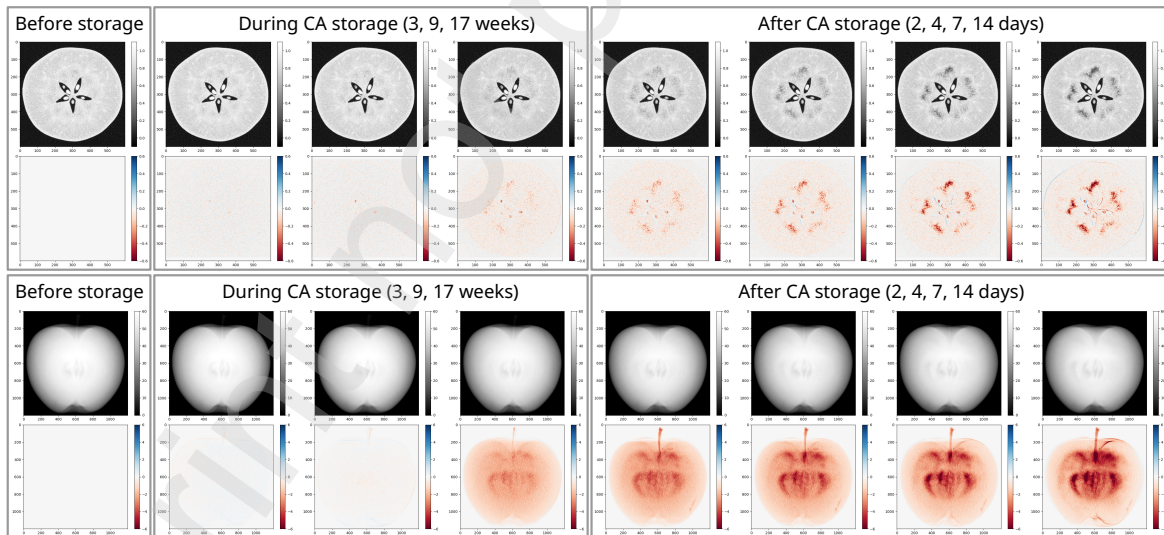


Figure 3: Top: Central slice of registered CT scans over time, and difference images showing the difference from the before storage scan. Bottom: Simulated radiographs of the same apple over time, and difference images showing the difference from the before storage radiograph.

307 4.2 Quantitative analysis of regional changes

308 Figure 4 shows how the whole apple porosity, change in whole apple porosity, inner apple porosity,
 309 and change in inner apple porosity relate to the browning score. The p-value of the one-way ANOVA
 310 test was highest on the whole apple porosity, and lowest on the change in inner apple porosity. The
 311 change in inner apple porosity also had the least overlap between the browning scores. It had a

312 statistically significant ($p < 0.05$) difference between scores 1, 2 and 3 (healthy, mildly brown and
 313 brown), and no significant difference scores 3 and 4 (brown and severely brown).

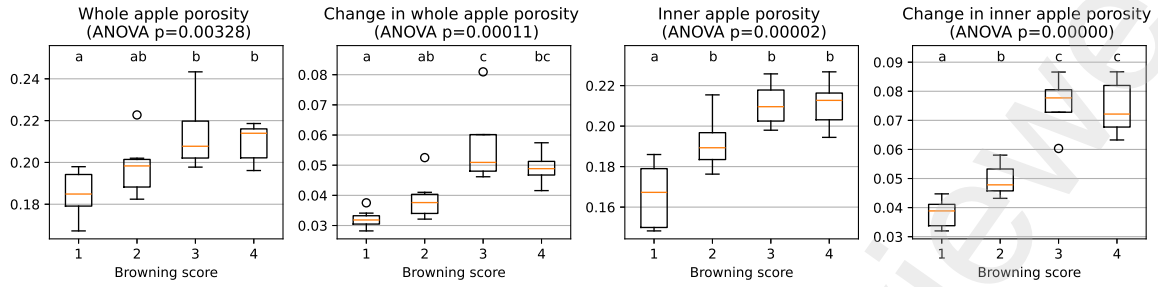


Figure 4: Boxplots of how four features related to porosity vary for each browning score. The orange line shows the median, the box shows the range between the first and the third quantile, and the whiskers show the range of values, except for outliers, which are shown as circles. Groups are statistically different ($p < 0.05$) according to a Tukey’s range test if they don’t share any letters (abc). The p-value above each boxplot corresponds to a one-way ANOVA test with the null hypothesis that the means were the same for all browning scores.

314 4.3 Classification for early detection

315 The results of the neural networks on the test-set are shown in Table 2. To put these results into
 316 context, if a classifier had learned to output the same score for all apples, the score with both the
 317 lowest MAE and the highest yes/no accuracy would be 2. Only outputting this score would result
 318 in an MAE of 0.9333 on the detection task and 1.0 on the prediction task, and a yes/no accuracy of
 319 0.667 on the detection task and 0.6 on the prediction task. All four neural networks outperform such
 320 a classifier, showing that they have learned to use the image data. The neural networks trained on CT
 321 slices performed better than the networks trained on radiographs in all cases. Combining the outputs
 322 of multiple input images also improved the results in most cases, resulting in a 100% detection and
 323 prediction of the presence of browning from CT scans. For the prediction task networks the validation
 324 set results were worse than the test-set results. The validation set MAE of the CT prediction network
 325 was 0.398 and 0.300 for separate and combined images respectively, and the yes/no accuracies were
 326 81.2% and 90.0%. The validation set MAE of the radiograph prediction network was 0.825 and 0.700
 327 for separate and combined images respectively, and the yes/no accuracies were 70.1% and 80.0%.
 328 The worst performing neural network was the radiograph prediction network. The training of this network
 329 also started overfitting earlier. The best MAE validation score was found at epoch 479, while for the
 330 other three networks, the best MAE validation score was found after more than 5000 epochs.

Table 2: Results of the neural networks on the test-set.

		Browning score MAE		Browning yes/no accuracy	
		Separate	Combined	Separate	Combined
CT slices	Detection	0.333	0.200	95.7%	100%
	Prediction	0.176	0.000	91.2%	100%
Radiographs	Detection	0.430	0.400	85.9%	86.7%
	Prediction	0.693	0.700	78.0%	80.0%

331 4.4 Longitudinally explainable deep learning

332 The neural network outputs on the zero and black baselines were far (14 or more) outside the 1-4
 333 range of expected scores for all networks except the CT prediction network. On that network, the
 334 black baseline had a score of 0.94 and the zero baseline had a score of 1.14. Table 3 shows the results
 335 of the evaluation of the longitudinal baseline. The score was within the 1-4 range for all images on
 336 all networks and the other properties were met on most images. Figure 5 shows examples of IG with
 337 a longitudinal baseline for all four networks on the same apple.

Table 3: Results of the evaluation of the longitudinal baseline.

		Healthy mean and std. dev.	Brown mean and std. dev.	Healthy and score 1	Brown and increasing
CT slices	Detection	1.00 ± 0.03	1.12 ± 0.23	100%	100%
	Prediction	1.07 ± 0.07	1.55 ± 0.30	100%	90%
Radiographs	Detection	1.14 ± 0.20	1.54 ± 0.36	90%	98%
	Prediction	1.29 ± 0.05	1.29 ± 0.07	100%	77%

5 Discussion

5.1 Image registration

The image registration method in this paper is easy to reproduce because it is completely described in Section 3.2, has publicly available code, and relies on free software libraries only. Therefore it is a good starting point for image registration in future longitudinal X-ray imaging studies.

5.2 Difference image visualizations

Image registration makes it easier to compare images by showing them in the same orientation. When showing 2D slices of a 3D volume it also helps in showing the same part of the volume (Muziri et al. 2016; Schut et al. 2024). Figure 3 shows that difference images have the additional advantage of higher visual contrast, especially on the simulated radiograph images.

5.3 Quantitative analysis of regional changes

Figure 4 showed that using a region of interest, and looking at changes over time both resulted in more discriminative features, and that these two approaches can be combined to derive even more discriminative features. Calculating the change between two measurements is only one way of combining data in a longitudinal dataset. It is also possible to perform statistical analysis using measurements of more than two days by using non-linear mixed-effects regression (Tijskens et al. 2015). For example, non-linear mixed-effects regression was used to derive a biological age for ‘Granny Smith’ apples based on color measurements (Tijskens et al. 2008). Applying longitudinally derived features in sorting machines would require storing data for individual products through the supply chain, which is an upcoming trend in industry (Stephan et al. 2013).

The relation between porosity and browning was studied before by Chigwaya et al. (2021) in ‘Fiji’ apples. They found no statistically significant difference in whole apple porosity between apples that developed browning and apples that did not. However, when the porosity was calculated only over the coreline region the difference was significant. In earlier research within the same project, core browning was studied using the same dataset of ‘Braeburn’ apples, but the apples for which no before-storage scan was available were also included. For browning scores being at least two apart (e.g. 1 and 3) the density was significantly different, but for adjacent scores (e.g. 1 and 2) it was not (Wood et al. 2024). In Section (4.2) significant differences were found for the change in inner apple porosity between scores 1, 2, and 3, showing that the approach of data analysis on regional changes can result in more discriminative features.

5.4 Classification for early detection

The separate radiographs prediction setup is most similar to what currently could be implemented in a sorting system. Apples are typically sorted right after they come out of storage, and about ten radiographs could be acquired per second with an acquisition time of 100 ms, which is similar to the throughput in a commercial sorting system. The setups that combined multiple CT slices served as an indicator for the best-case performance if there is no limit on acquisition time. Moreover, research is ongoing to increase the throughput of CT scanners (Morton et al. 2009; De Schryver et al. 2016; Schut et al. 2022), so real-time CT scanning might become available in the future. The fact that a browning detection accuracy of 100% was reached on the combined CT slices setups suggests that

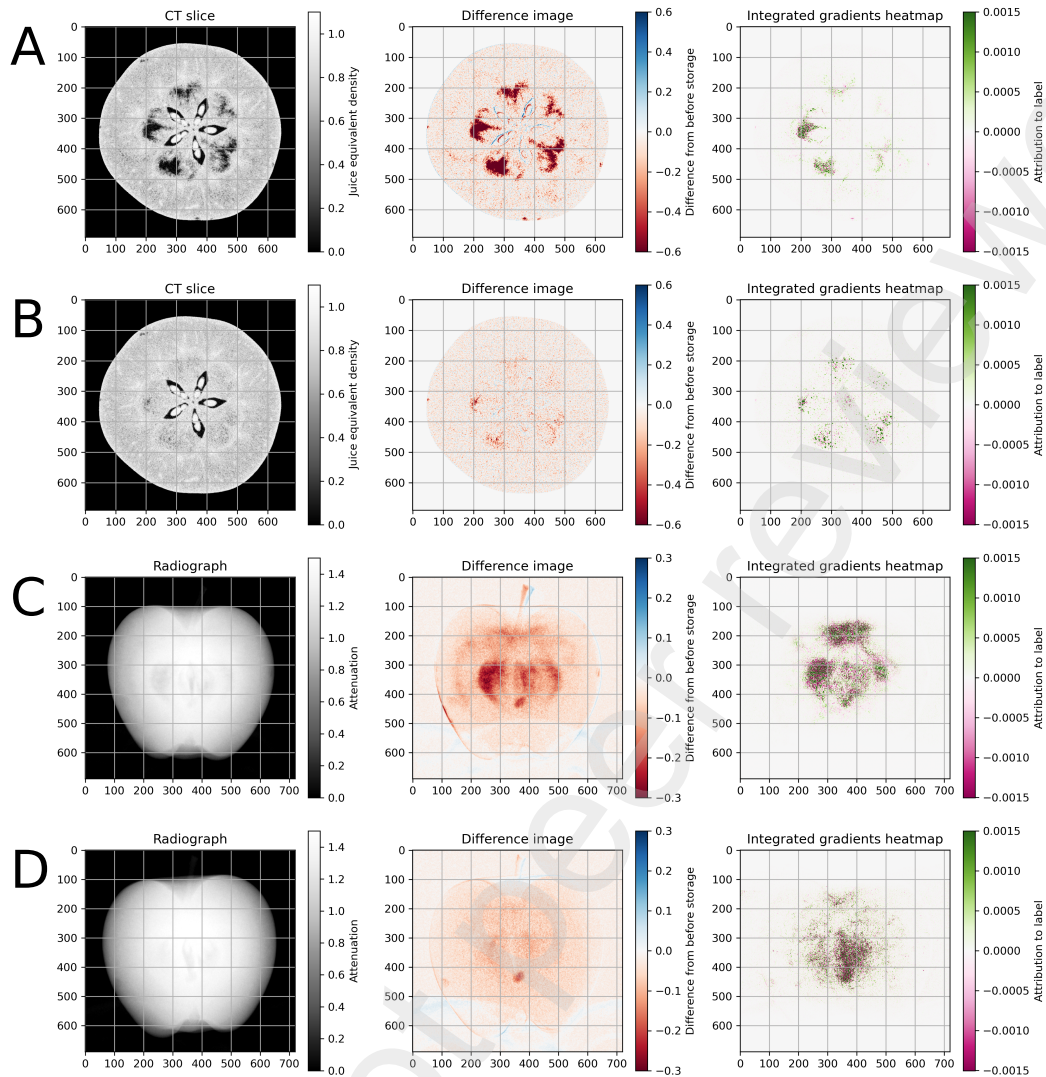


Figure 5: Examples of IG heatmaps with a longitudinal baseline A: Result on the CT detection network. B: Result on the CT prediction network. C: Result on the radiograph detection network. D: Result on the radiograph prediction network. All images were calculated on the same apple with browning score 4.

377 both detection and prediction of browning are possible if sufficiently high-quality X-ray images are
 378 available.

379 In our dataset, the grower, growing season, cultivar and storage conditions were the same for all
 380 apples. ‘Braeburn’ apples are typically very sensitive to browning disorders, but this also varies
 381 with orchard (Neuwalde et al. 2014), and weather conditions (McCormick et al. 2021; Wood et al.
 382 2022), which would need additional testing. On one hand, having more varied data could worsen
 383 the detection performance. On the other hand, more apples could be scanned to train the neural
 384 networks, which could improve the detection performance. The somewhat limited number of apples
 385 used for neural network training could also explain why the validation set results were better than the
 386 test-set results on the prediction task neural networks because the test and validation sets consisted
 387 of just 10 apples in the prediction task.

388 The result that browning can be detected on a single CT slice agrees with our earlier results (Wood et
 389 al. 2024). The IG heatmap is also similar to the void segmentation images that were used for browning
 390 detection in that paper. Tempelaere et al. (2024) also trained neural networks for detecting browning
 391 from CT scans and radiographs and achieved more than 95% accuracy with both. Our experiments

392 extend upon these earlier works by scoring the severity of the browning on a 1-4 scale instead of
393 yes/no classification, and by performing prediction of future browning from just-out-of-storage images.
394 Another difference is that Tempelaere et al. (2024) used multiple CA storage conditions, with all apples
395 from the browning-inducing CA storage conditions developing severe browning and all other apples
396 remaining healthy. In our work, all apples were stored in the same CA conditions, and the resulting
397 smaller changes between the brown and healthy apples are more challenging to classify and more in line
398 with industry. J. He et al. (2024) compared dark-field and conventional transmission radiographs and
399 suggested dark-field radiography is more suited to detect internal soft-tissue disorders like browning.
400 Dark-field radiographs can not be simulated from transmission CT scans, but grating-based setups
401 can capture transmission, dark-field, and phase-contrast CT scans at the same time (Bech et al. 2010)
402 which could be used to acquire longitudinal multimodal CT datasets, adding another dimension for
403 comparing setups.

404 5.5 Longitudinally explainable deep learning

405 Many baselines for IG have been suggested in the literature and the choice of baseline highly impacts
406 the outcome of IG (Sturmfels et al. 2020; Mamalakis et al. 2023). Most research using IG has been
407 done on classification networks, but in this paper, a regression network was used. Classification
408 networks have a softmax or sigmoid activation function at the output, which are bounded to the
409 $[0, 1]$ range and have a high level of saturation (Rakitienskaia and Engelbrecht 2015), meaning that
410 they map most of their inputs to values close to either zero or one. The regression networks used in
411 this paper have a linear activation function at the output, which doesn't have this property. This
412 could explain why the black and zero baselines did not meet the evaluation criteria on three of the
413 four neural networks in this paper (Section 4.4). Furthermore, Sturmfels et al. (2020) showed that
414 IG is blind to image features with the same color as the baseline. In the case of the X-ray images
415 of apples, areas with browning show up as darker spots, with very brown spots in CT being almost
416 black. Therefore a black baseline would be blind to these spots, which is undesirable. IG with a
417 longitudinal baseline is blind to areas that did not change over time. There is background noise in
418 all four difference images in Figure 5, but this does not show up in the heatmaps, showing that the
419 neural networks are not activating on the background. Table 3 showed that most heatmaps did not
420 contradict the fact that browning can only increase. This evaluation is not just an evaluation of the
421 baseline, but also of the neural network (e.g. an untrained network with a perfect baseline image
422 would not pass it).

423 The heatmaps in Figure 5 highlighted regions where browning was expected to occur. However,
424 within these regions, there are both positive and negative values, often in neighboring voxels. It is
425 unclear why the negative values appear within regions of interest, but it is a common phenomenon in
426 IG heatmaps, so we don't expect it to be related to the apples. The standard approach to remove this
427 phenomenon is to visualize the absolute value of the heatmap (Smilkov et al. 2017; Adebayo et al.
428 2018). However, with that approach the heatmaps lose the completeness property, making them less
429 interpretable. Another approach, called XRAI (Kapishnikov et al. 2019), segments the image into
430 small regions and postprocesses the IG heatmap so that each region has only one score. This removed
431 the neighboring positive and negative values in the examples shown in that paper.

432 6 Conclusions

433 Longitudinal CT datasets quantify the internal state of agricultural products in 3D over time, making
434 them very suitable for studying the progression of postharvest disorders. We presented a workflow
435 for developing early detection systems using longitudinal CT data, and we showcased the workflow
436 on a dataset of 'Braeburn' apples developing core browning. To align the CT scans of the same
437 apple an image registration method was developed based on SimpleITK (Section 3.2), that registered
438 the CT scans up to voxel precision (Figures 3 & 5). The development of core browning during
439 and after CA storage on CT slices and radiographs was shown in detail (Figure 3). The method of
440 difference images improved the visibility of the disorder, especially on the radiographs. The change
441 in inner apple porosity was significantly different for apples with no browning, mild browning, and
442 moderate browning (Figure 4). Calculating this feature only over the affected region (inner apple) and
443 calculating the change between two time points made this feature more discriminative. Furthermore,

our results suggest that by using neural networks on X-ray images browning can be scored on severity and future browning can be predicted from just-out-of-storage scans (Table 2). To find the optimal scanning setup to apply on a sorting line, many setups can be simulated from the same longitudinal CT dataset (Section 3.5). IG heatmaps were calculated to show how the neural network interpreted the images (Figure 5). Because we used a longitudinal baseline the heatmaps answer the research question “How much did the changes in density from before storage affect the browning score?” We conclude that by combining image registration and longitudinal CT scanning powerful data analysis techniques are made possible. Most of the presented methods use no apple-specific properties, so they should be applicable to other agricultural products or to longitudinal CT datasets from other fields.

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Data availability

Data will be made available on request.

Appendices

A Number of images in the train, validation, and test sets

Table A.1: Division of apples into the train, validation, and test sets and the resulting number of CT slices and radiographs.

	Train set			Validation set			Test set		
	Apples	CT slices	Radiographs	Apples	CT slices	Radiographs	Apples	CT slices	Radiographs
Detection	45	5550	21600	15	1848	7200	15	1884	7200
Prediction	32	3922	15360	10	1240	4800	10	1248	4800

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